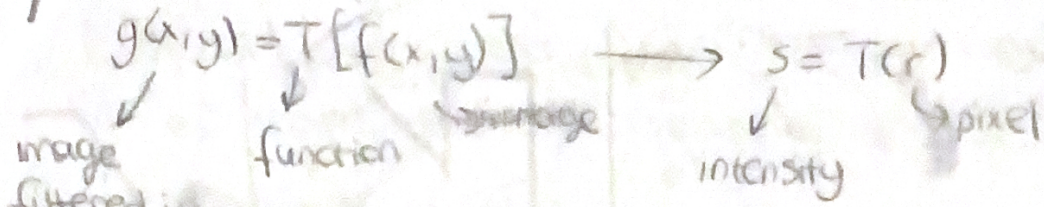


Spatial Domain Filtering



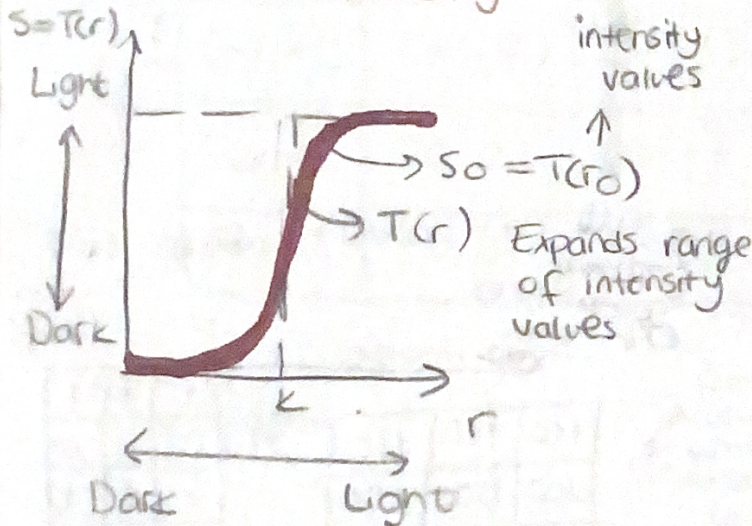
→ Single Pixel Operations → Negative Image
→ Contrast Stretching

→ Neighborhood Operations → Averaging Filter
→ Median Filtering

→ Geometric Spatial Functions → Scaling → $\begin{bmatrix} c_x & 0 & 0 \\ 0 & c_y & 0 \\ 0 & 0 & 1 \end{bmatrix}$
→ Rotation → $\begin{bmatrix} \cos \theta & \sin \theta & 0 \\ -\sin \theta & \cos \theta & 0 \\ 0 & 0 & 1 \end{bmatrix}$
→ Translation → $\begin{bmatrix} 1 & 0 & 0 \\ 0 & 1 & 0 \\ t_x & t_y & 1 \end{bmatrix}$

Intensity Transformations

Contrast Stretching



Thresholding Function

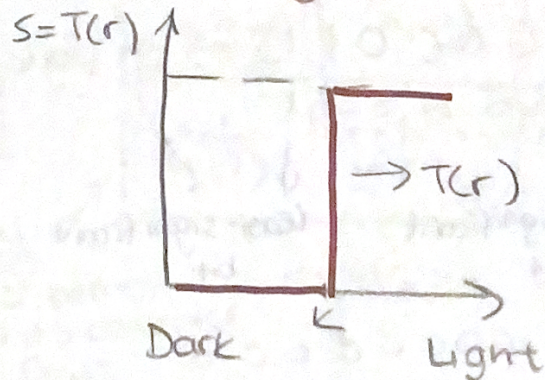
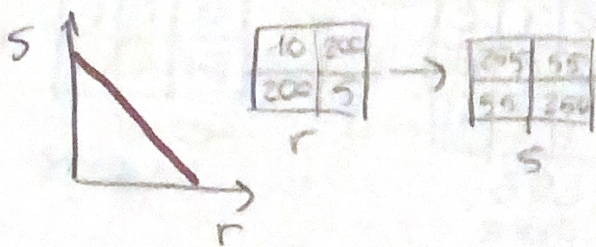


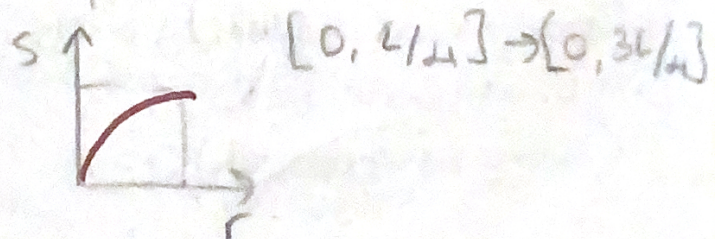
Image Negatives

$S = L - 1 - r$



Log Transformation

- Increases the brightness
 - $S = c \log(1+r)$
- Expand the values of dark pixels & compress bright pixels.



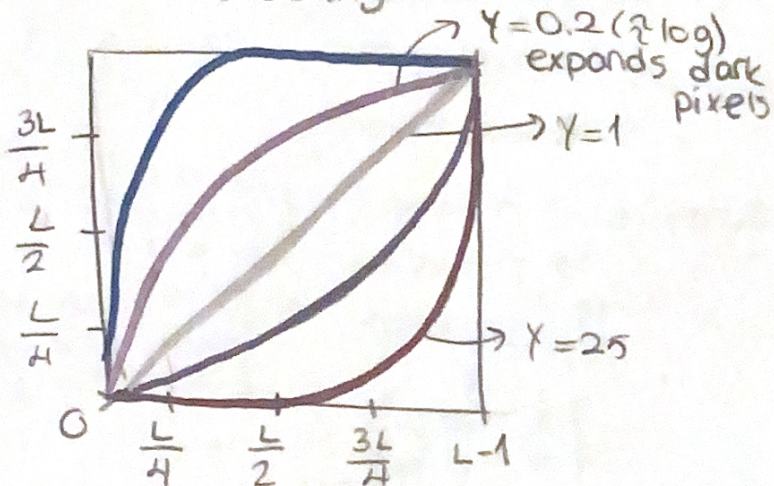
Power Law (Gamma) Transform

$$s = cr^\gamma \rightarrow c, \gamma > 0$$

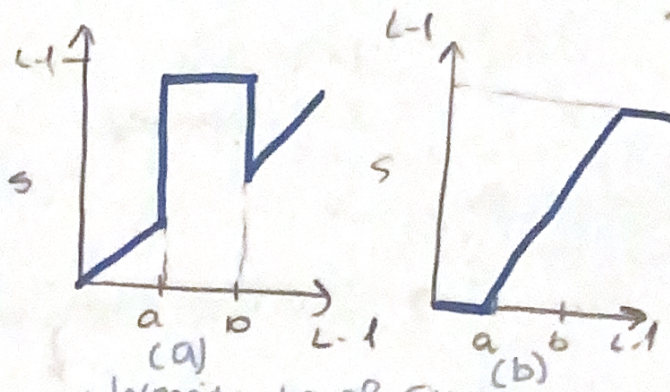
$0 < \gamma < 1 \rightarrow$ expands dark pixels

$\gamma > 1 \rightarrow$ compresses dark pixels

$c = 1 \rightarrow$ identity



Piecewise Linear Transformation



\rightarrow Intensity Level Slicing

Highlight specific range of intensities in an image.

(a) Displays only one value in range of interest and rest is black (converts to binary)

(b) Brightens a range s_1 leave the rest.

Bit Plane Slicing

1 1 0 0 0 0 1 0 \rightarrow Bit plane

8 7 6 5 4 3 2 1

\downarrow
most significant bit

\downarrow
least significant bit

0 \rightarrow 0 0 0 0 0 0 0 0

intensity \uparrow

! All other intensities

255 \rightarrow 1 1 1 1 1 1 1 1
4 msb

Store less planes (with highest significance) to save memory.

Reconstruction \rightarrow Multiply pixels of n th plane by 2^{n-1}
(binary bit \rightarrow decimal)

\rightarrow We can convert images to bit planes.

ex: 3 bit image

110	111	110
000	000	000
001	101	101

1	1	1
0	0	0
0	1	1

MSB plane

0	1	0
0	0	0
1	1	1

LSB plane

1	1	1
0	0	0
0	0	0

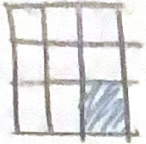
center bit plane

Spatial Filtering

Linear Spatial Filtering

Sum of products between image f & filter kernel w .

$$g(x,y) = w(-1,-1) f(x-1,y-1) + w(-1,0) f(x-1,y) + \dots + w(0,0) f(x,y) + \dots + w(1,1) f(x+1,y+1)$$



$$g(x,y) = \sum_{s=-a}^a \sum_{t=-b}^b w(s,t) \cdot f(x+s,y+t)$$

Spatial Correlation & Convolution

Correlation: Moving center of a kernel over an image & computing sum of products at each location

Measurement between similarity of two signals

$(x,y) \rightarrow$ any point in the image

w

$(-1,-1)$	$(-1,0)$	$(-1,1)$
$(0,-1)$	$(0,0)$	$(0,1)$
$(1,-1)$	$(1,0)$	$(1,1)$

kernel coefficients

f

$(x-1, y-1)$	$(x-1, y)$	$(x-1, y+1)$
$(x, y-1)$	(x, y)	$(x, y+1)$
$(x+1, y-1)$	$(x+1, y)$	$(x+1, y+1)$

pixel values under kernel when it's centered on (x,y)

Correlation: $(w \cdot f)(x,y) = \sum_{s=-a}^a \sum_{t=-b}^b w(s,t) f(x+s,y+t)$

Convolution: Measurement of effect of one signal on another

$(w * f)(x,y) = \sum_{s=-a}^a \sum_{t=-b}^b w(s,t) f(x-s,y-t)$

flip the kernel on both sides

When kernel is symmetrical, correlation = convolution

Filters

Prewitt Filter

$$\begin{bmatrix} -1 & 0 & 1 \\ -1 & 0 & 1 \\ -1 & 0 & 1 \end{bmatrix}$$

→ Vertical edges

Convolving Prewitt will give you:

$$\nabla I = \frac{\nabla I}{\partial x} + \frac{\nabla I}{\partial y}$$

↑ horizontal change ↑ vertical change

$$\begin{bmatrix} -1 & -1 & -1 \\ 0 & 0 & 0 \\ 1 & 1 & 1 \end{bmatrix}$$

→ Horizontal edges

Sobel Filter

$$\begin{bmatrix} +1 & 0 & -1 \\ +2 & 0 & -2 \\ +1 & 0 & -1 \end{bmatrix}$$

$$\begin{bmatrix} +1 & +2 & +1 \\ 0 & 0 & 0 \\ -1 & -2 & -1 \end{bmatrix}$$

used in edge detection.

Smoothing

We can do →

$$\begin{bmatrix} 1 & 1 & 1 \\ 1 & 1 & 1 \\ 1 & 1 & 1 \end{bmatrix} / 9$$

which is brute force

Better solution →

Gaussian Smoothing

$$\begin{bmatrix} 8 & 9 & 8 \\ 9 & 10 & 9 \\ 8 & 9 & 8 \end{bmatrix}$$

Closer ones should be smoothed less

$$G(i,j) = \frac{1}{2\pi\sigma^2} e^{-\frac{|i^2+j^2|}{2\sigma^2}}$$

Histogram Processing

Distribution of intensity values.

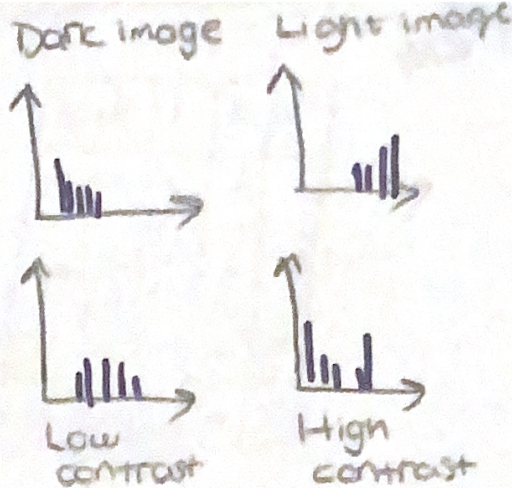
$$h(r_k) = n_k \quad \text{for } k = 0, 1, \dots, L-1$$

\downarrow intensity level \swarrow number of pixels in f with intensity r_k

$$p(r_k) = \frac{h(r_k)}{MN} = \frac{n_k}{MN}$$

\downarrow estimates of probabilities of intensity levels \downarrow row \downarrow column

estimates of probabilities of intensity levels



Histogram Equalization

Used to improve contrast.

Cumulative Distribution Func $\rightarrow \sum_0^{255} \frac{n_j}{n}$ $P_r(v_k) = \frac{n_k}{n}$ \swarrow probability density function

What we do $\rightarrow s_i = cdf_i \cdot (L-1)$

1	1	1	1
1	5	6	1
1	6	5	1
1	1	1	1

$$Pr_1 = 12/16 \quad cdf_1 = 12/16$$

$$Pr_5 = 2/16 \quad cdf_5 = 14/16$$

$$Pr_6 = 2/16 \quad cdf_6 = 16/16$$

$$s_1 = \frac{12}{16} \cdot 16 = 12$$

$$s_5 = \frac{14}{16} \cdot 16 = 14$$

$$s_6 = 1 \cdot 16 = 16$$

Histogram Matching

Modifying images based on the contrast of another one.

1. First equalize the histogram of both images. $(L-1) \sum_{j=0}^k Pr(r_j)$
2. Map each pixel of image A to B $\rightarrow G(z_q) = s_k$
3. Modify A according to B $\rightarrow z_q = G^{-1}(s_k)$

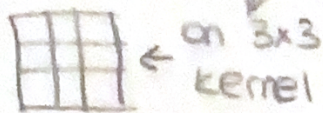


Spatial Filtering

Linear Spatial Filtering

Sum of products between image f & filter kernel w

$$g(x,y) = w(-1,-1)f(x-1,y-1) + w(-1,0)f(x-1,y) + \dots + w(0,0)f(x,y) + \dots + w(1,1)f(x+1,y+1)$$

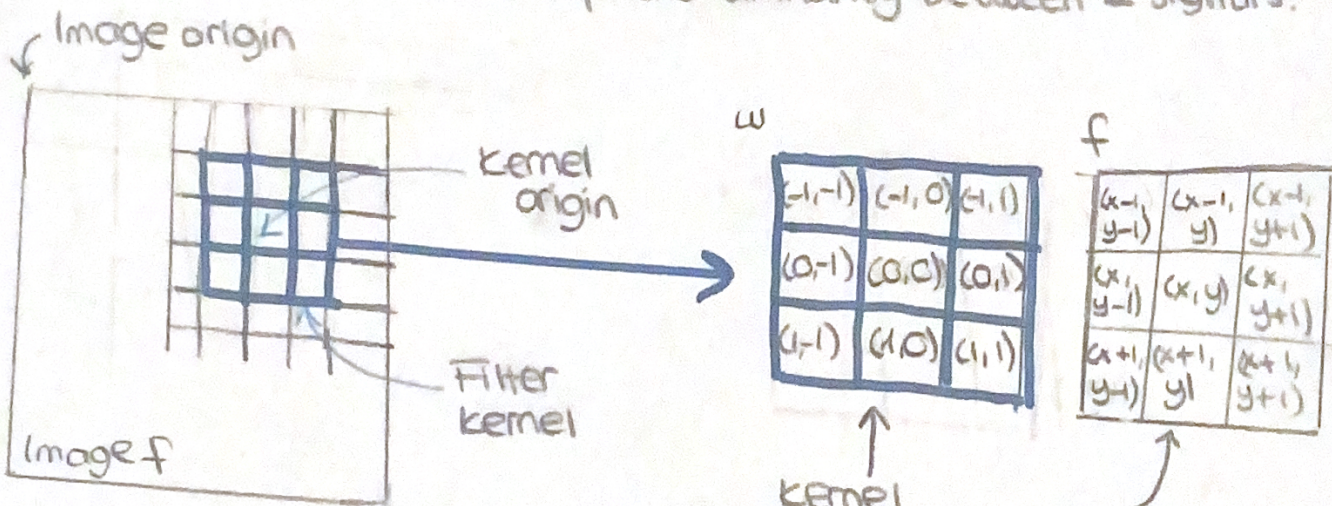


$$* g(x,y) = \sum_{s=-a}^a \sum_{t=-b}^b w(s,t) \cdot f(x+s, y+t)$$

Spatial Correlation & Convolution

- **Correlation:** Moving center of a kernel over an image and computing sum of products at each location.

It's a measurement of the similarity between 2 signals.



$(x,y) \rightarrow$ any point in the image

kernel coefficients $w(-1,-1) \dots$

Pixel values under kernel when it is centered on (x,y)

- Correlation Formula $\rightarrow (w * f)(x,y) = \sum_{s=-a}^a \sum_{t=-b}^b w(s,t) f(x+s, y+t)$
- Convolution: Measurement of effect of one signal on the other signal.

Convolution Formula: $(w * f)(x,y) = \sum_{s=-a}^a \sum_{t=-b}^b w(s,t) f(x-s, y-t)$

1	2	3
4	5	6
7	8	9

Correlation

9	8	7
6	5	4
3	2	1

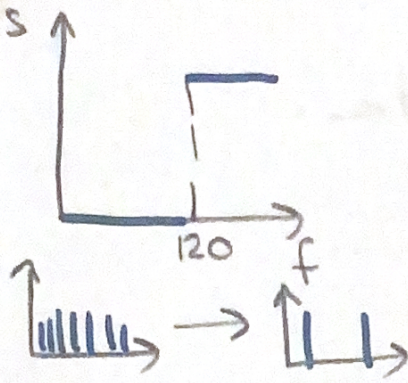
Convolution

Kernel w : $\begin{matrix} 1 & 2 & 3 \\ 4 & 5 & 6 \\ 7 & 8 & 9 \end{matrix}$

- When kernel is symmetrical
Correlation = convolution

→ Image Binarization

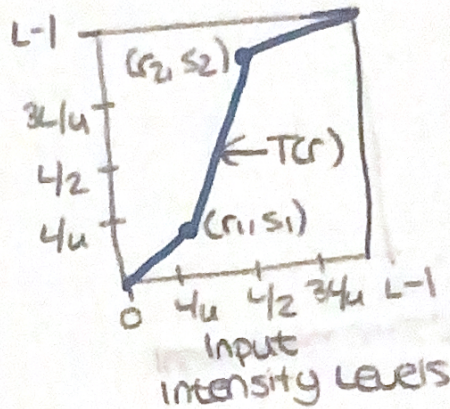
Makes images B & W



Output Intensity Levels

→ Contrast Stretching

Expands range of intensity levels so that it comes to an ideal range.

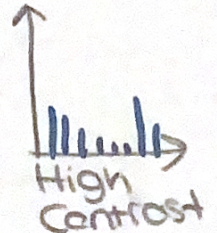
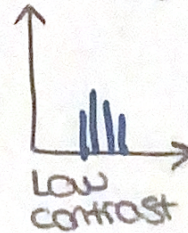
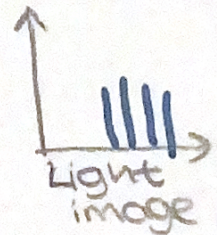


Histogram Processing

Distribution of intensity values.

→ $h(r_k) = n_k$ for $k = 0, 1, \dots, L-1$
 ↓ intensity level ↘ number of pixels in f with intensity r_k

→ $p(r_k) = \frac{h(r_k)}{MN} = \frac{n_k}{MN}$
 ↓ estimates of probs of intensity levels
 row ← column



Histogram Equalization

Used to improve contrast.

Cumulative Distr. Func → $\sum_0^{255} \frac{n_j}{n}$ $Pr(r_k) = \frac{n_k}{n}$
 ↘ probability density function

What we do → $s_i = cdf_i \cdot (L-1)$

ex

1	1	1	1
1	5	6	1
1	6	5	1
1	1	1	1

$Pr_1 = 12/16$ $cdf_1 = 12/16$

$s_1 = \frac{12}{16} \cdot 255$

$Pr_5 = 2/16$ $cdf_5 = 14/16$

$s_2 = \frac{14}{16} \cdot 255$

$Pr_6 = 2/16$ $cdf_6 = 16/16$

$s_3 = \frac{16}{16} \cdot 255$

PDF → CDF → Equalization

Spatial Operations

Single Pixel Operations

Alter the intensity of its pixels individually.

$$S = T(z)$$

↳ operation

Geometric Transformations

Modify spatial arrangement of images. Consists of following

1. Spatial transformation of coordinates
2. Intensity interpolation that assigns intensity values to spatially transformed pixels.

Transformation coordinates can be expressed as:

$$\begin{bmatrix} x' \\ y' \end{bmatrix} = T \begin{bmatrix} x \\ y \end{bmatrix} = \begin{bmatrix} t_{11} & t_{12} \\ t_{21} & t_{22} \end{bmatrix} \begin{bmatrix} x \\ y \end{bmatrix}$$

↓
pixel coord.
in
transformed
image

↓
these values
determine the
type of operation

↳ pixel
coordinates
in original
image

ex// $(x', y') = (x/2, y/2)$ → shrinks the original image by half.

Affine Transformations

- Scaling
 - Translation
 - Rotation
 - Sheer
- } geometric ops

Neighborhood Operations

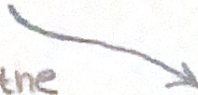
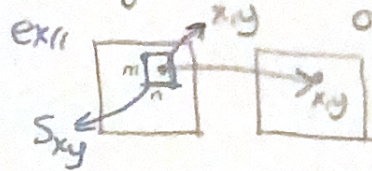
S_{xy} → set of coordinates of a nbhd

ex// Compute the average value of the pixels in the input image with coordinates in the set S_{xy} → Burs

$$g(x, y) = \frac{1}{mn} \sum f(r, c)$$

↓
generated
image

↓
row & col
coordinate
of pixels in
 S_{xy}



ex// Identity → $\begin{bmatrix} 1 & 0 & 0 \\ 0 & 1 & 0 \\ 0 & 0 & 1 \end{bmatrix}$

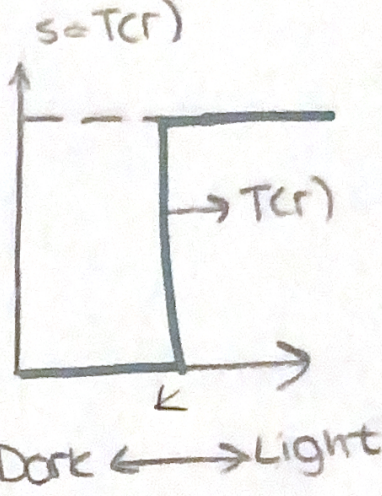
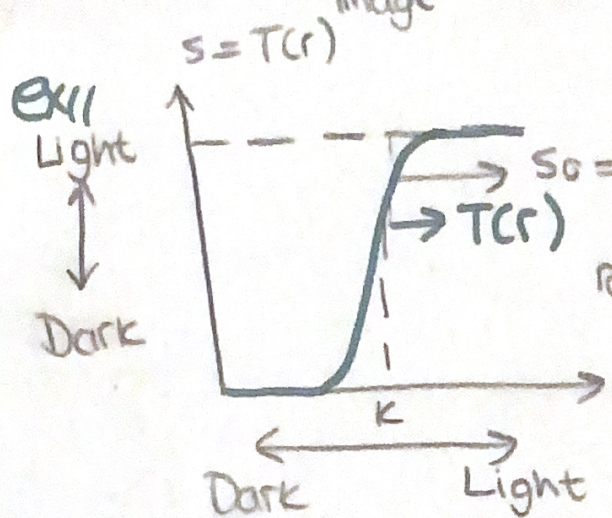
Scaling → $\begin{bmatrix} c_x & 0 & 0 \\ 0 & c_y & 0 \\ 0 & 0 & 1 \end{bmatrix}$

Rotation → $\begin{bmatrix} \cos \theta & -\sin \theta & 0 \\ \sin \theta & \cos \theta & 0 \\ 0 & 0 & 1 \end{bmatrix}$

Intensity Transformations & Spatial Filtering

$$g(x, y) = T[f(x, y)]$$

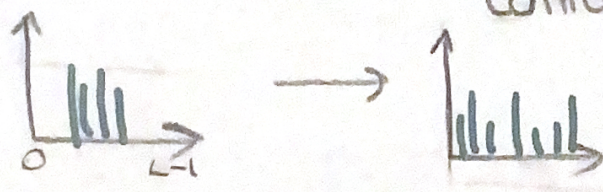
$g(x, y)$ → output image
 T → a func.
 $f(x, y)$ → input image



Contrast Stretching

Thresholding Function

Increasing Contrast



Basic Transformations

→ Image Negatives

$$s = L - 1 - r$$

10	200	Neg. →	245	55
200	5		55	250

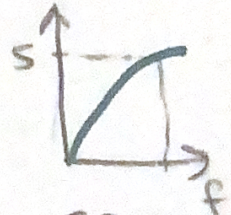
f s



→ Log Transformation

Increases the brightness.

$$s = c \log(1+r)$$

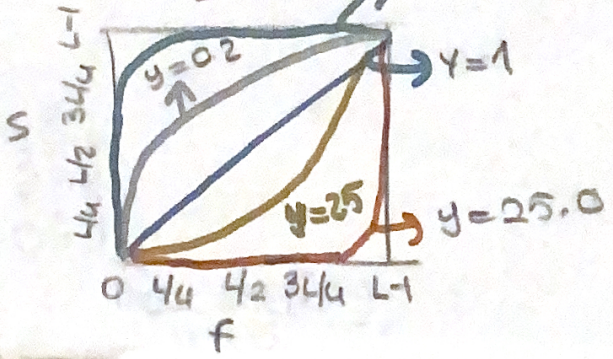


Expand the values of dark pixels in the image & compress higher level values.

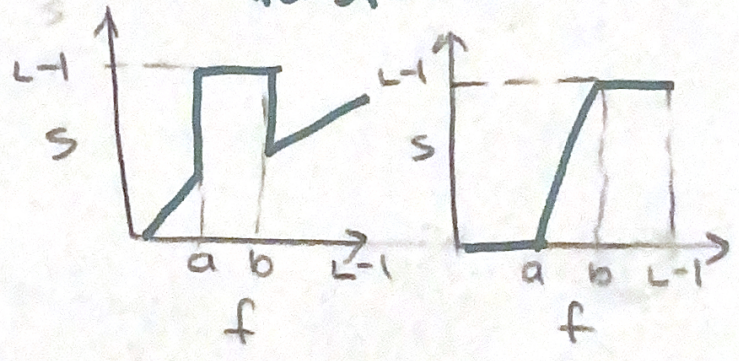
eg. $[0, L/4] \rightarrow [0, 3L/4]$

→ Power Law (Gamma) Tr.

$$s = cr^\gamma$$



→ Piecewise Linear Transformation



Histogram matching

Modifying one image based on the contrast of another one.

1. First equalize the histogram of both images $(L-1) \sum_{j=0}^k pr(r_j)$
2. Map each pixel of image A to B. $G(z_q) = s_k$
3. Modify A according to B. $z_q = G^{-1}(s_k)$

ex 11

0	2	1	3	4
1	3	4	3	3
0	1	3	1	4
3	1	4	2	0
0	4	2	4	4

Image A

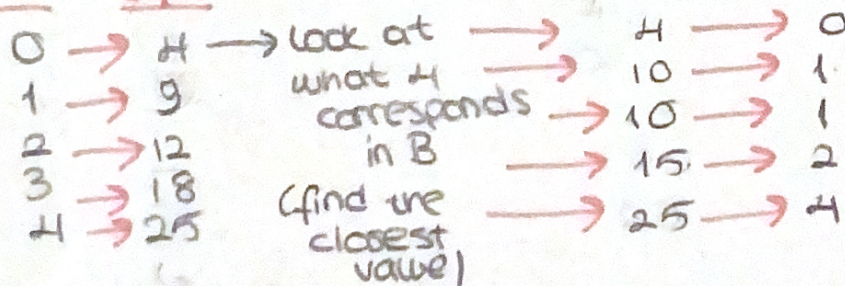
2	1	2	1	0
3	3	2	4	4
1	3	2	4	4
0	0	3	2	1
1	3	1	4	0

Image B
(Target)

Pixel Value	freq Histogram	Equalized Hist (cdf)
0	4	4
1	5	9
2	3	12
3	6	18
4	7	25
0	4	4
1	6	10
2	5	15
3	5	20
4	5	25

Map each pixel in A based on it's equalized histogram, to the value of B.

A eq.A



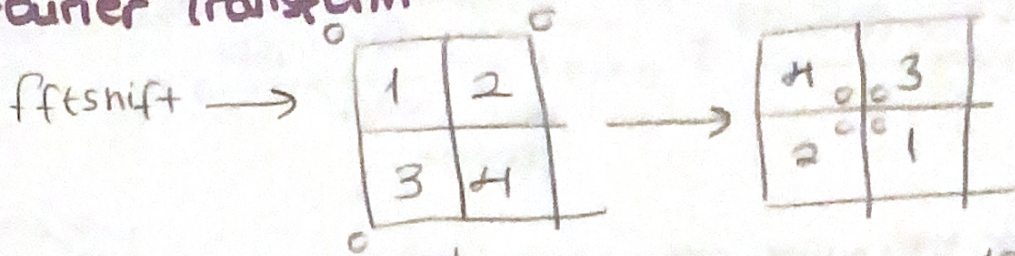
0	1	1	2	4
1	2	4	2	2
0	1	2	1	4
2	1	4	1	0
0	4	1	4	4

Modified A

* Changes:

- 0 → 0
- 1 → 1
- 2 → 1
- 3 → 2
- 4 → 4

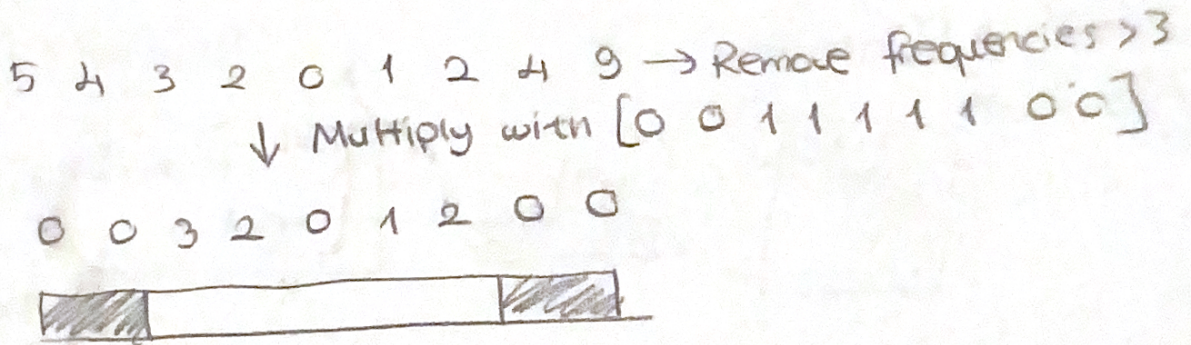
Fourier Transform



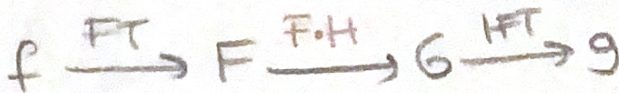
\downarrow
we want to put zeros in the middle

\hookrightarrow what does zero freq mean? zero change.
High freq \rightarrow high change.

Smooth by removing high frequency. (details of the image)
If we want to remove details (smooth) we remove high frequencies.

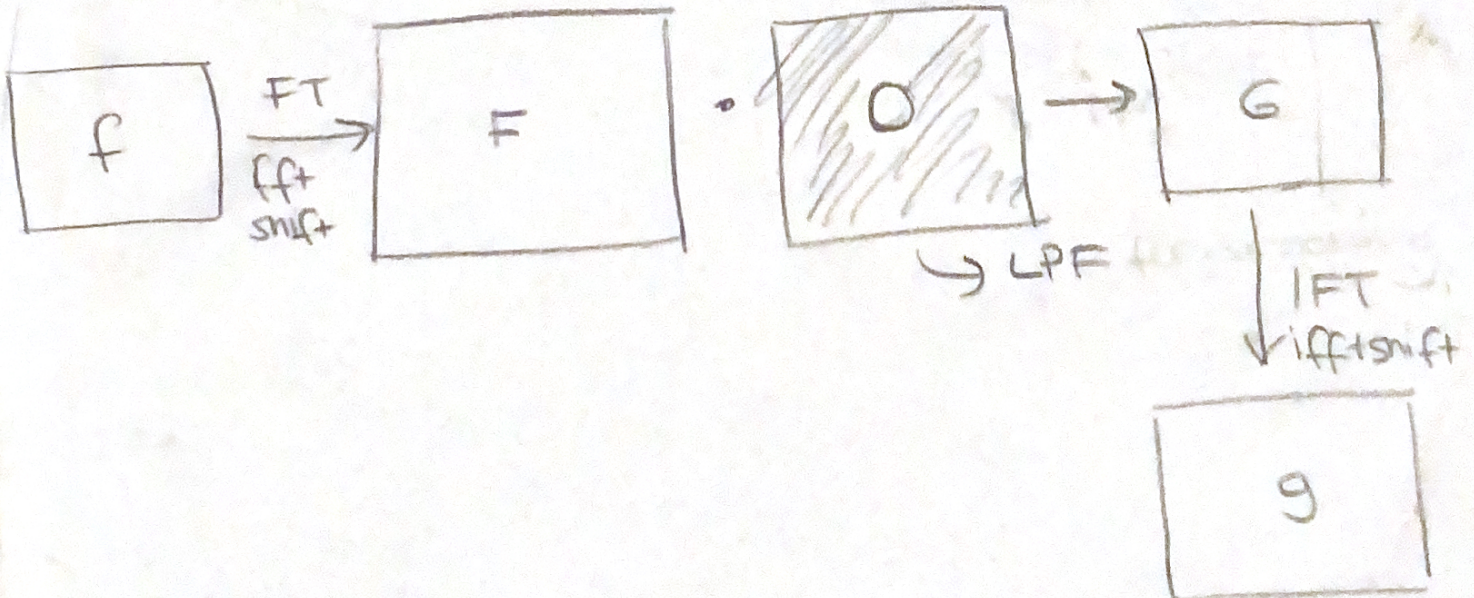


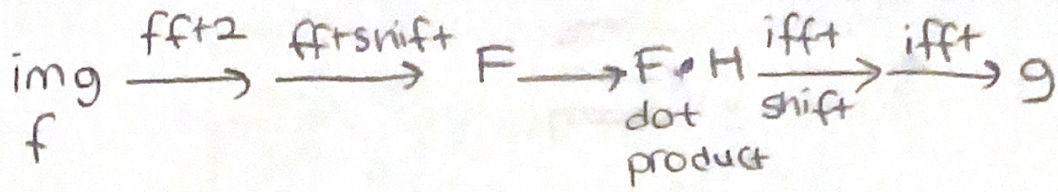
With convolution theorem $f * h \leftrightarrow F \cdot H$
 spatial domain \leftrightarrow freq domain



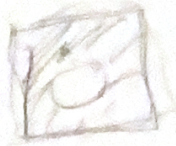
\hookrightarrow with FT we can do filtering in freq domain (better for isolating frequencies)

In 2D if we have

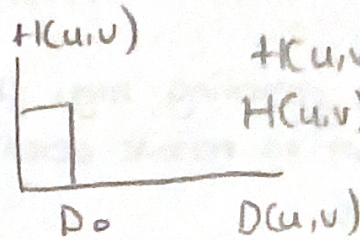
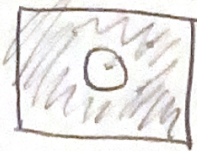




Smaller the white circle more blur (in LPF)



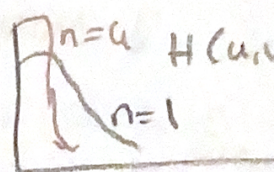
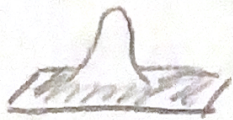
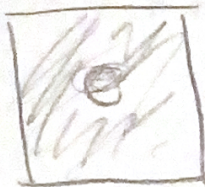
→ Ideal Filter



$$H(u,v) = 1 \text{ if } D(u,v) < D_0$$

$$H(u,v) = 0 \text{ if } D(u,v) > D_0$$

→ Butterworth

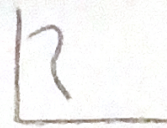
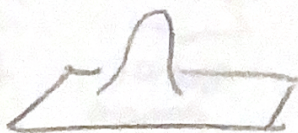
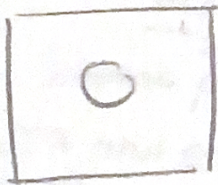


$$D(u,v) = \sqrt{(u - M/2)^2 + (v - N/2)^2}$$

$$H(u,v) = \frac{1}{(1 + (D(u,v)/D_0)^{2n})^{1/n}}$$

Kernel
order

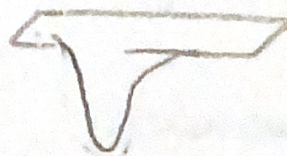
Gauss



$$D(u,v) = \exp\left(-\frac{D(u,v)^2}{2D_0^2}\right)$$

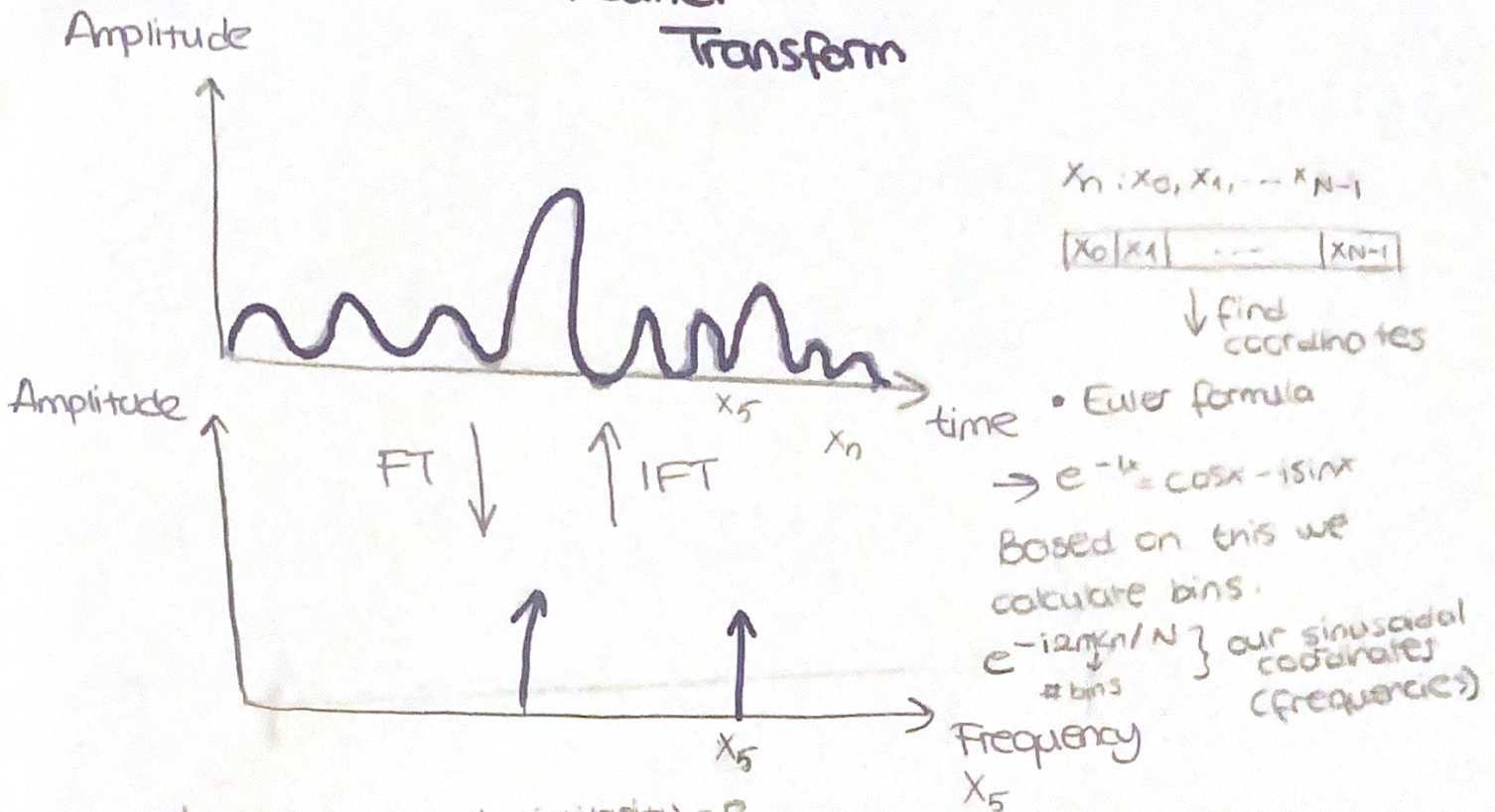
cutoff freq

HPF = 1 - LPF →

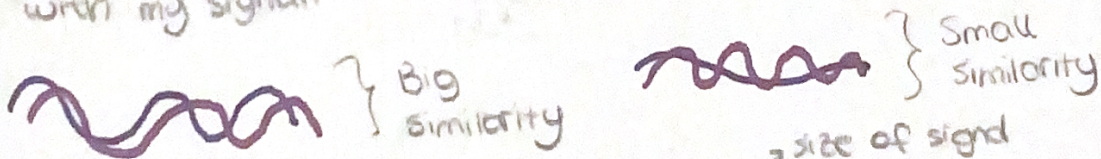


$D_0 \uparrow$ HPF edge'ler kalir
 $D_0 \downarrow$ LPF blur \uparrow

Fourier Transform



I have to check similarity of every coordinate (for different k 's) with my signal.



FT for one bin only $\rightarrow X_k = \sum_{n=0}^{N-1} x_n e^{-2\pi i k n / N}$

$N-1 \rightarrow$ size of signal

We need 2 for loops to calculate all k 's

* def myDFT(x_n):

N = len(x_n)

for k=0:N-1

x_k = 0

for n=0:N-1

$$x_k = x_k + \overbrace{x_n[n+1]}^{\text{element (signal)}} * \exp(-2 * i * \pi * n * k / N)$$

output[k+1] = x_k

We'll calculate this for:

	n=0	n=1	n=2	n=3
k=0	00	01	02	03
k=1	10	11	12	13
k=2	20	21	22	23
k=3	30	31	32	33

→ FFT reduces complexity from n^2 to $n \log n$.

Discrete Fourier Transform in 2D

1D → k in $M \times X$

2D → u, v in $M, N \times F, F$

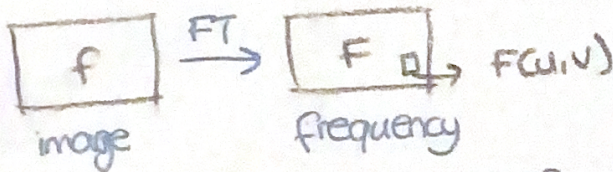
$$F(u, v) = \sum_{x=0}^{M-1} \sum_{y=0}^{N-1} f(x, y) e^{-i 2\pi \left(\frac{ux}{M} + \frac{vy}{N} \right)}$$

↓
→ pixel of the frequency transformed image

↓
original signal

→ u & v are the frequencies

→ A frequency in an image corresponds to change in an image



How to calculate fourier in 2D?

def myDFT2D(f)

for $u=0:M-1$

for $v=0:N-1$

for $x=0:M-1$

for $y=0:N-1$

output[u+1, v+1] = output[u+1, v+1] +

f[x+1, y+1] * exp(-2*pi*i*(x+u/M +

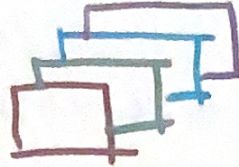
y+v/N))

COLORS

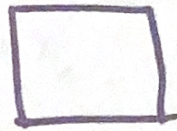


Color Image
RGB

Each layer is 8 bits/px
3 layers = 24px



RGBA Image with Alpha (transparency)
4 layers = 32px



Gray Level Image
8 bits/px



Binary Image
1 bit/px

ex // RGB Image \rightarrow 8 bits/pixel = 1 byte

600x480
Size (MB) = $\frac{3 \text{ bytes} \times 600 \times 480}{1024} / 1024$
 \rightarrow Byte \rightarrow KB \rightarrow MB

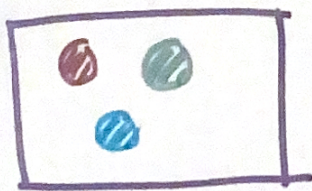
1 byte = 8 bits
1 MB = $\frac{1024 \times 1024}{1024}$ byte
1 MB = $\frac{1024 \times 1024}{1024}$ kilobyte

ex // Binary Image
600x400
1 bit/px

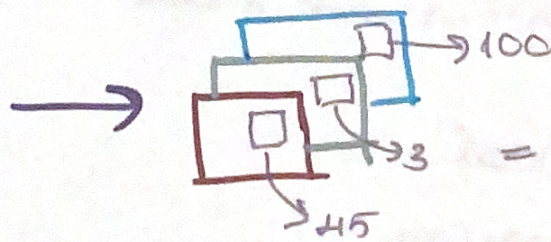
$\frac{600 \times 400 \times 1}{8} / 1024 / 1024$
 \rightarrow Bit \rightarrow Byte \rightarrow KB \rightarrow MB

ex // HD Image (1920x1080)
RGB

$\rightarrow 3 \text{ bytes} \times 1920 \times 1080 / 1024 / 1024$

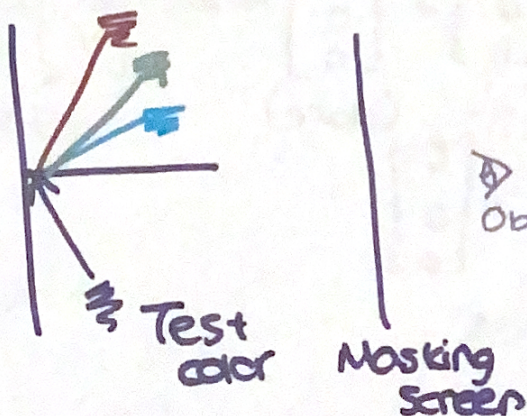


Pixel



= we need a palette to answer!
390 \rightarrow B
700 \rightarrow R

Colorimeter



UV VS IR

To define 3D perceptual space, observers match color of a given wavelength \rightarrow lambda by mixing three other pure wavelengths
phosphors of color TVs & other CRTs do not emit pure R, G or B light of a single wavelength.

CIE Chromaticity Diagram

3D → 2D color space

$$x + y + z = 1$$

weights

$$x = \frac{x}{x+y+z}$$

$$y = \frac{y}{x+y+z}$$

$$z = 1 - x - y$$

Color models

* RGB
color monitors
cameras

Emitted light

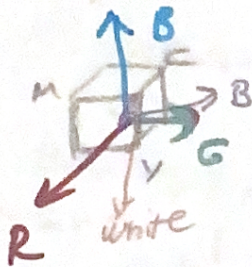
RGB Color model

Based on a cartesian system

* CMYK
(cyan magenta
yellow black)
printers

Reflected light

* HSI
(Hue, saturation,
illuminance)
for human



R: 0-255 byte
G: 0-255 byte
B: 0-255 byte

Emitted light

ex

>> $r = \text{zeros}(100, 100, 3)$

>> $I(r, i, 1) = 255 \rightarrow$ only red image

>> $I(:, :, 2) = 255 \rightarrow$ made it yellow

>> $I(i, i, 3) = 255 \rightarrow$ made it white

the color layer itself
is white

CMYK Color Model

Expresses reflected light

$$\begin{bmatrix} C \\ M \\ Y \end{bmatrix} = \begin{bmatrix} 1 \\ 1 \\ 1 \end{bmatrix} - \begin{bmatrix} R \\ G \\ B \end{bmatrix}$$

$$\text{if } \begin{bmatrix} R \\ G \\ B \end{bmatrix} = \begin{bmatrix} 0 \\ 0 \\ 0 \end{bmatrix} \text{ then } \begin{bmatrix} C \\ M \\ Y \end{bmatrix} = \begin{bmatrix} 1 \\ 1 \\ 1 \end{bmatrix}$$

K = Black

(black)

black

$$\text{if } \begin{bmatrix} R \\ G \\ B \end{bmatrix} = \begin{bmatrix} 1 \\ 1 \\ 1 \end{bmatrix} \text{ then } \begin{bmatrix} C \\ M \\ Y \end{bmatrix} = \begin{bmatrix} 0 \\ 0 \\ 0 \end{bmatrix}$$

white

white

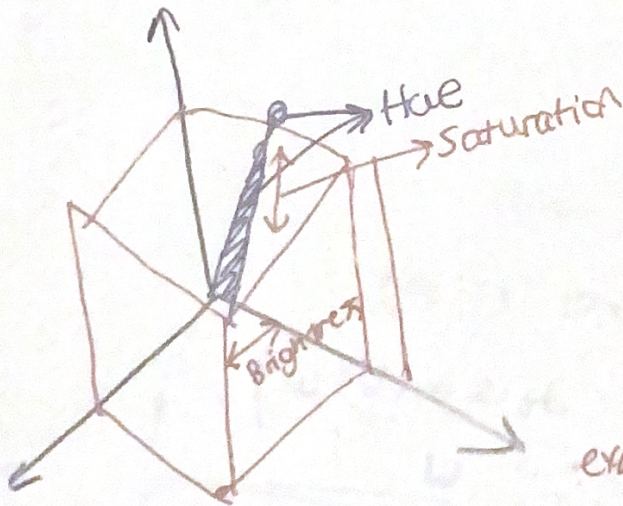
if $\begin{bmatrix} R \\ G \\ B \end{bmatrix} = \begin{bmatrix} 1 \\ 0 \\ 0 \end{bmatrix}$ then $\begin{bmatrix} C \\ M \\ Y \end{bmatrix} = \begin{bmatrix} 0 \\ 1 \\ 1 \end{bmatrix}$

HSI/HSV Color Model

Suitable for humans.

- * Hue \rightarrow Pure color (RGB CMYK)
- * Saturation \rightarrow Measure of purity, degree of which a pure color is diluted by white light
- * Luminance / Value / Intensity \rightarrow Brilliance of color

HSI Geometric Representation



\rightarrow Choose color, then saturation then brightness.

$$I_{HSV} = rgb2HSV(I)$$

$I_{HSV}(i, :, 1)$ (hue)
 \rightarrow colors, red is at the end

$$[m \ n \ c] = \text{size}(I)$$

ex) for $i=1:m$

for $j=1:n$

if $(I_{HSV}(i, j, 1) < 0.95$

$I_{HSV}(i, j, 1) = 0;$

ex)

if $I_{HSV}(i, j, 1) < 0.90:$

$$I(i, j, i) = \frac{I(i, j, 1) + I(i, j, 2) + I(i, j, 3)}{3}$$

3

\rightarrow convert to grayscale

(everything but red)

ex)

\rightarrow brightness

$I_{HSV}(i, :, 3) = I_{HSV}(i, :, 3) - 0.5 \rightarrow$ becomes darker

$$I_{new} = HSV2RGB(I_{HSV})$$

Medical Imaging

Medical Imaging Devices

Computed Tomography Scanner

- X-ray Scanner
- Magnetic Resonance Impedance Scanner (MRI)

PET Scanner

Ultrasound devices

X-Rays

- Short wavelength electromagnetic waves
- Wavelength is between 10^{-1} - 10 nm
- X-ray photons have a lot of energy
- It is dangerous → can produce chemical damage on molecules
↳ knock particles out of atoms

High freq → high energy → heat

Image is produced based on absorption of x-rays to different tissues / bones of the body.

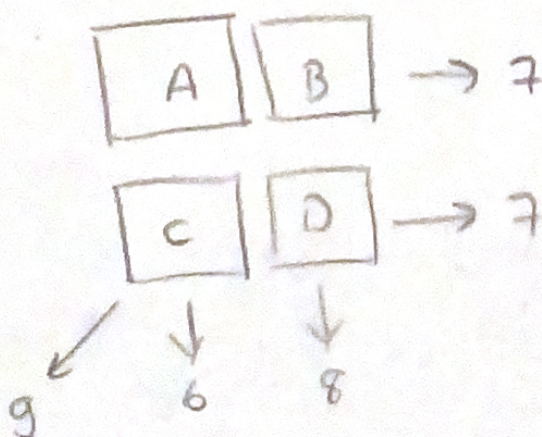
Computed Tomography

Allows us to see what's inside of human body without dissecting it.

It allows us to produce 2D cross sections of an object using X-rays.

→ How the image is produced by multiple projections!

We have horizontal, vertical & diagonal sums of following image



$$A + B = 7$$

$$A + C = 6$$

...

Sums simulate x-ray absorptions of the image.

MRI CT Scanner

→ In CT Scan (an X-ray) images are not clear because they're based on absorption (It is good for bones, sometimes tissue)

→ MRI is based on protons

→ Into the body they have arbitrary positions

→ When we apply a strong magnetic field, protons are aligned with magnetic field, when radiofrequency pulse is applied, some of them gets activated. When pulse ends, activation ends & relaxation time T_1 is measured.

Because protons belong to H_2O (Hydrogen) it works better in tissues

Ultrasound Devices

Subsound

Ultrasound

→ Ultrasound is a sound we can't hear. (Audible → 20-18000 Hz)

It's greater than 20kHz. In medical imaging it's 1-15 MHz.

Lower Frequency ↓ Better penetration ↑ Less resolution (3 MHz)

Higher Frequency ↑ Worst penetration ↓ Higher resolution (12 MHz)
(we don't miss tissues)

- Development of fetus
 - Evaluation of blood flow
 - Detection of tumors
- } can be seen
(using doppler effect)

Medical Imaging

Formats & Algorithms

Dicom

→ Digital imaging communication in medicine (an image standard)
Has header & data part. Header → Info about patient & scanner

Hounsfield Unit

A unit describe the attenuation of X-rays inside the human body.

$$HU = \frac{\mu_x - \mu_{H_2O}}{\mu_{H_2O}} \times 1000$$

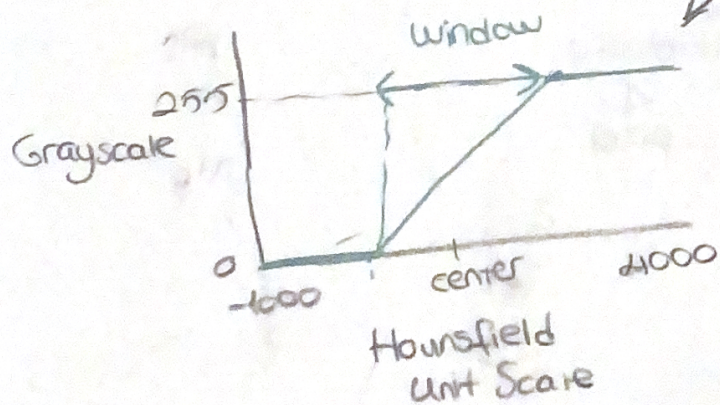
↙
attenuation coefficient
related to radiodensity
of material

↘ amount of transparency to the
passage of X-rays through
material.

$$HU_{H_2O} = 0 \quad \mu_{air} = 0 \rightarrow HU_{air} = -1000$$

HU is used in CT scanners.

In DICOM we store data in a range larger than 0-255 how we can display a wider range of values → Map for region we would like to display.



Volume Rendering

Technique for 3D visualization

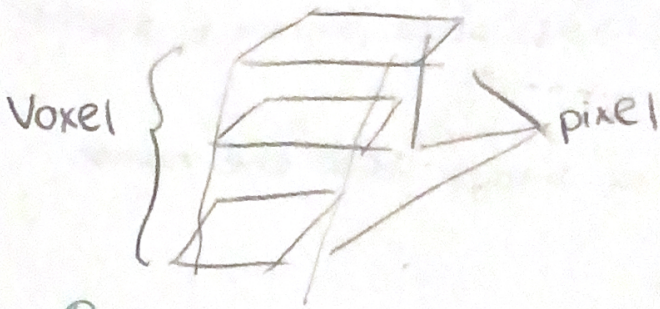
3D viz is hard due to → unclear borders between organs
↳ unclear elements inside organs

Instead of trying to separate structure, display all of them based on intensity values as 3D image

→ At beginning we have 2D CT scans.

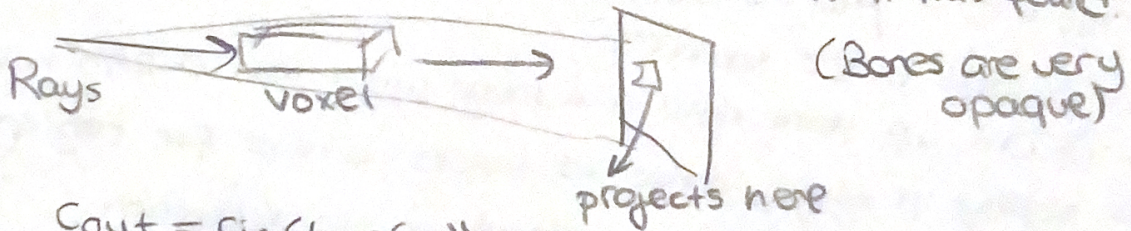
→ Then we define a voxel (volume element) → 3D pixel created from a pixel of an image belonging to a computed tomography scan.

We want opacity & color



Ray Casting

- Popular method to visualize voxel models
- Ray goes to 3D grid & resulted pixels take into account all the opacities & color of voxels it has found.



$$C_{out} = C_{in} (1 - a(x_i)) + c(x_i) a(x_i)$$

↓ ↓ ↓
outgoing opacity intensity
ingoing of pixel of pixel
intensity